



# Radiopharmaceutical Therapy (RPT) Dosimetry

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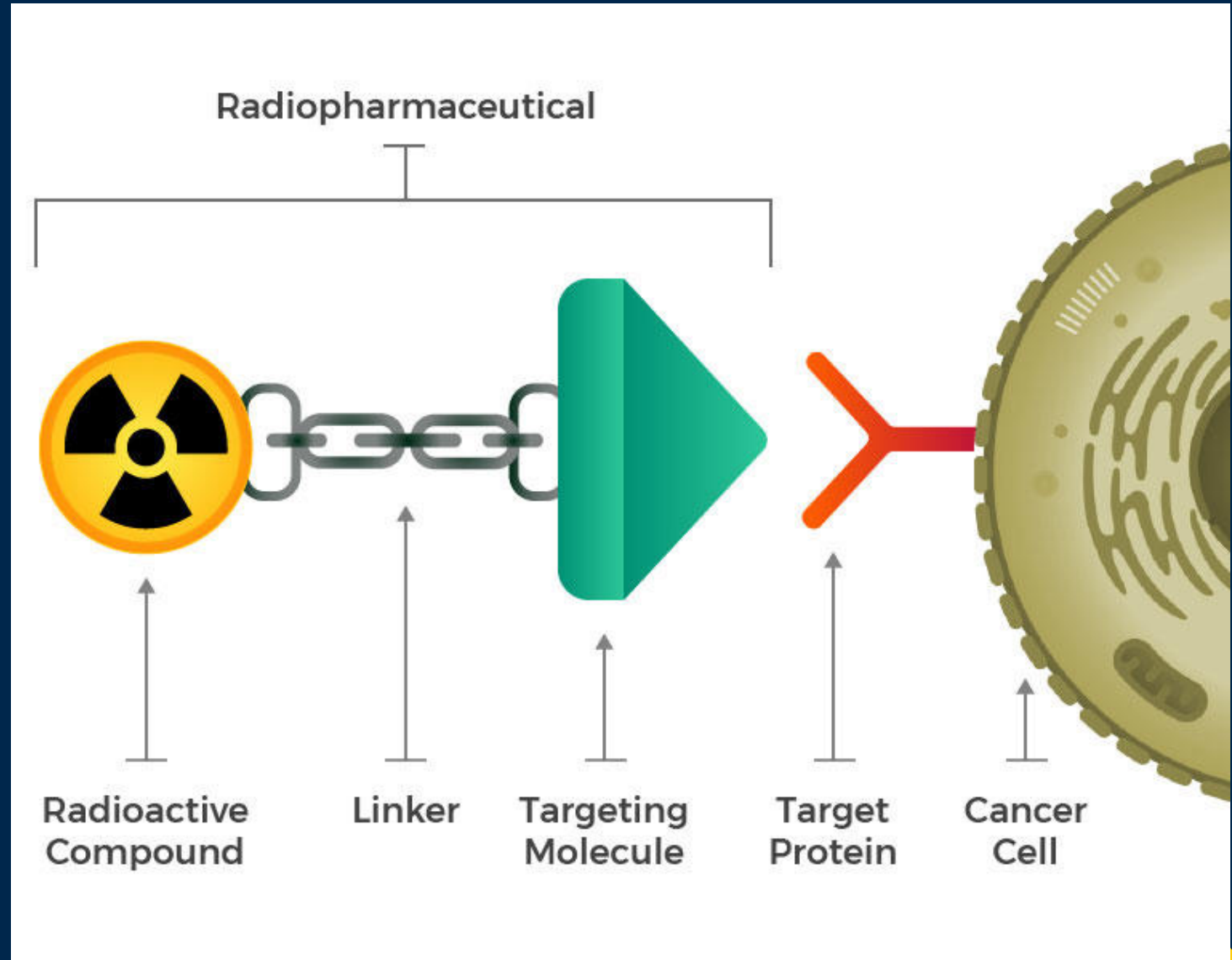
*Joint DOE / NIH Workshop - Advancing Medical Care through Discovery in the Physical Sciences Workshop Series:  
Radiation Detection. Session 4 - Cameras, Detectors for Therapeutics*

# Disclosures

- Yuni Dewaraja
  - Grant support from Varian
  - Software support from MLM Software, Inc
  - Software support from Siemens Molecular Imaging
  - Consultant for MLM Software, Inc.

# Radiopharmaceutical therapy (RPT)

- Also referred to as internal emitter therapy, radionuclide therapy, ...
- Radiopharmaceuticals: consist of a radioactive molecule, a targeting molecule, and a linker that joins the two
  - $^{177}\text{Lu}$ -PSMA , DOTATATE
  - Radioiodine therapy: the radioisotope (  $^{131}\text{I}$ ,  $^{124}\text{I}$  or  $^{123}\text{I}$ ) can be directly mediated by the sodium-iodide symporter in the thyroid cells.
  - Radioembolization: intra-arterial administration of Y-90 microspheres



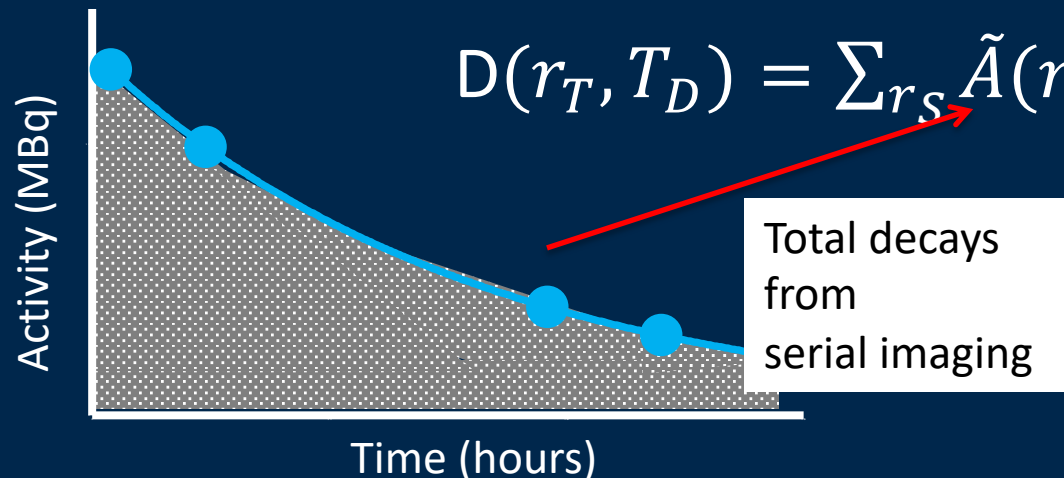
*Credit: National Cancer Institute*

# Radiopharmaceutical Therapy

- Current: Fixed activity (“one dose fits all”) or weight-based
  - Convenient, but variability in pharmacokinetics & anatomy not considered
  - Potential for under-treatment or over-treatment
- Desired: Absorbed dose guided treatment planning
  - Adjust activity to keep absorbed dose to critical organ  $<$  MTD.
  - Adjust to deliver therapeutic absorbed dose to lesion at acceptable toxicity
- Why Change?
  - With fixed activity promising tumor control, but poor complete response and survival rates
  - Low/mild toxicity, but are we underdosing most patients?
  - Potential for improved efficacy with dosimetry guided treatment

# Absorbed Dose Estimation in RPT: Main Steps

- Image Acquisition usually at multi time points for kinetics
  - Pre-therapy usually with surrogate or post-therapy directly
- Image Reconstruction, Quantification, Partial Volume Correction
- Image Registration
- Organ/lesion Segmentation
- Time - activity fitting
- Absorbed dose estimation. MIRL schema widely used

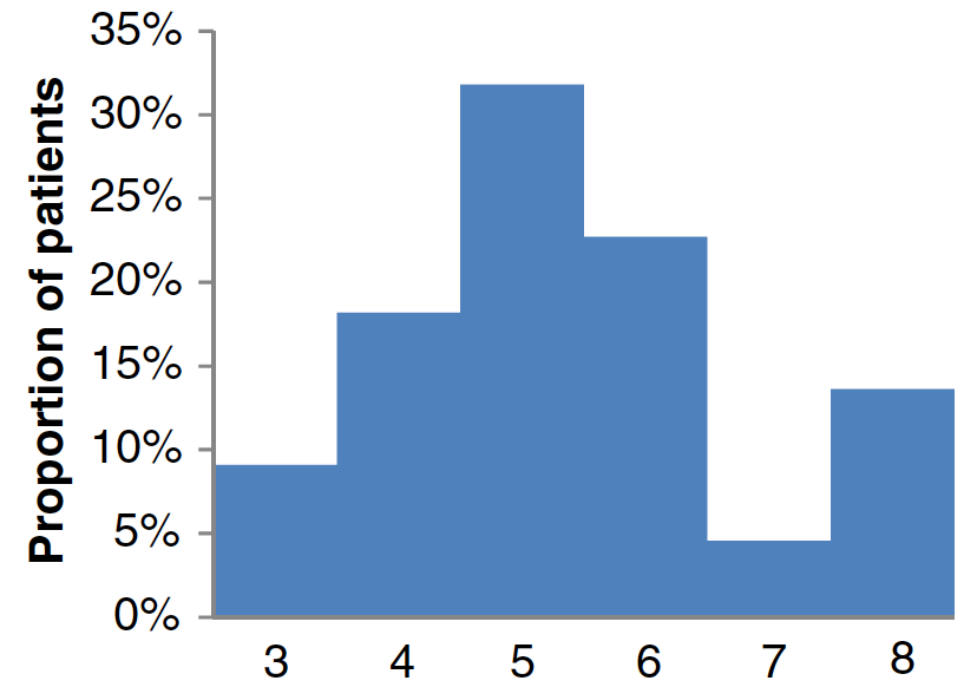
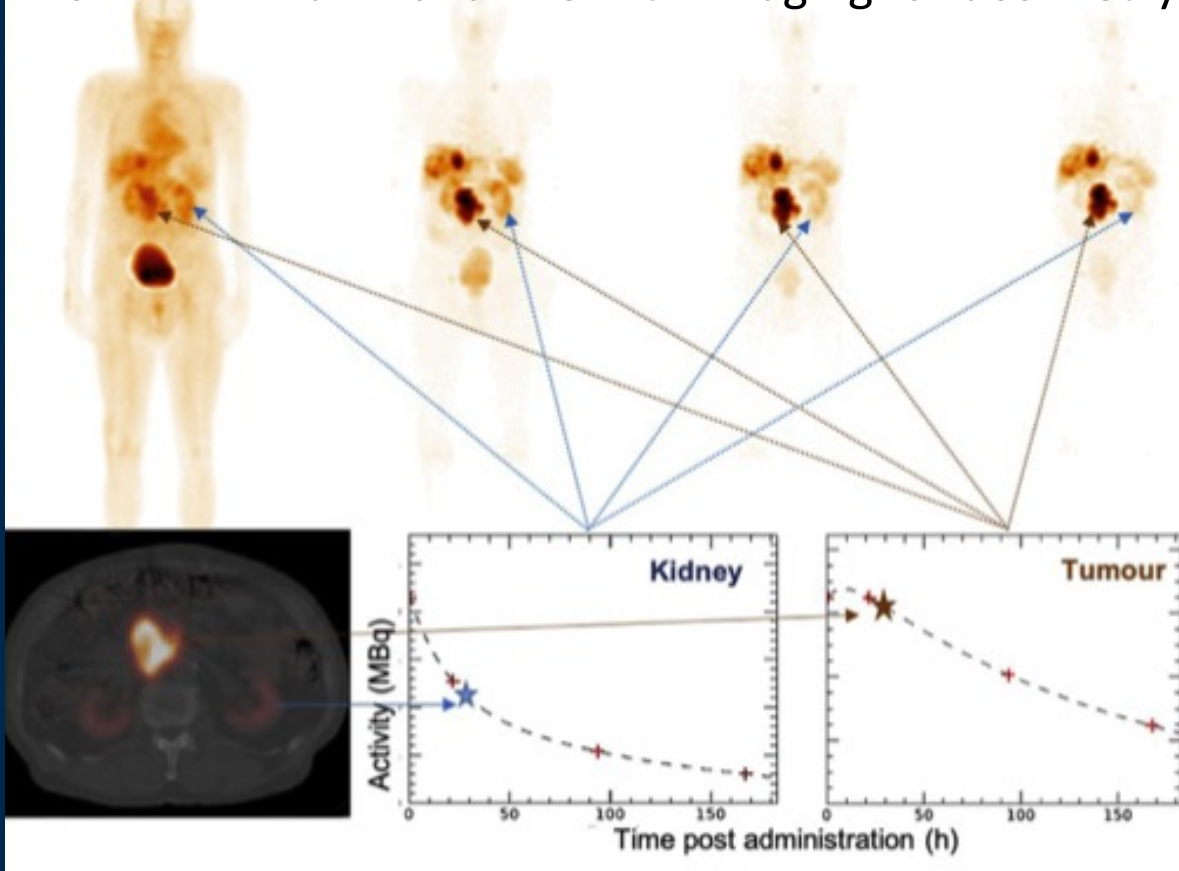


Absorbed dose to target per transformation in source. S-values can be at organ/sub-organ/voxel/cellular levels

# Example showing value of patient specific dosimetry: $^{177}\text{Lu}$ DOTATATE Trial

- Current standard: 4 cycles at 7.4 GBq/cycle
- Trial: As many cycles without exceeding kidney dose limit (MTD 27 Gy BED)
- Demonstrated: Cycles can be increased in most patients w/o reaching MTD

ILUMINET Trial: Planar + SPECT imaging for dosimetry



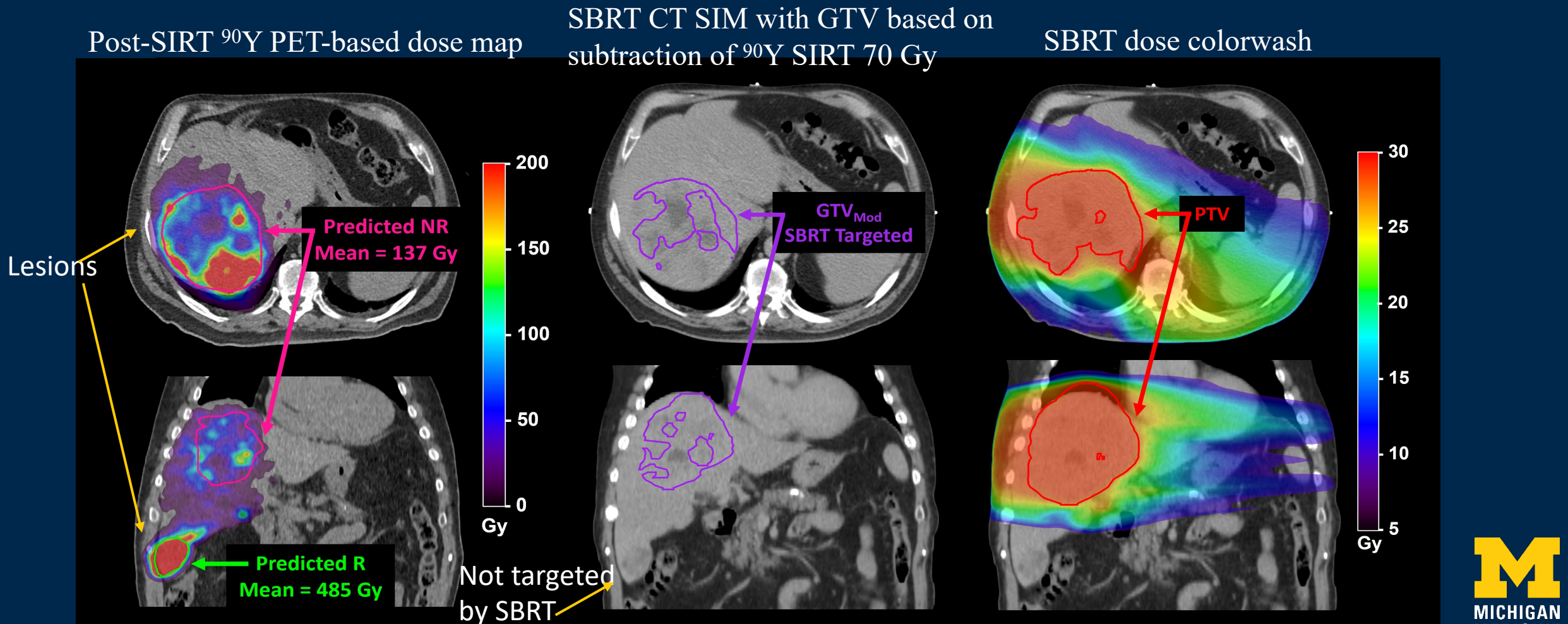
# of cycles within the protocol specified  
BED and AD limits



# Value of patient specific dosimetry: U of Mich combined $^{90}\text{Y}$ SIRT + SBRT

Current: HCC lesions targeted by  $^{90}\text{Y}$  selective internal radiation therapy or external radiotherapy

Trial:  $^{90}\text{Y}$  PET absorbed dose map used to identify underdosed regions and boost with SBRT



# RPT: Why dosimetry guided treatment is not standard practice

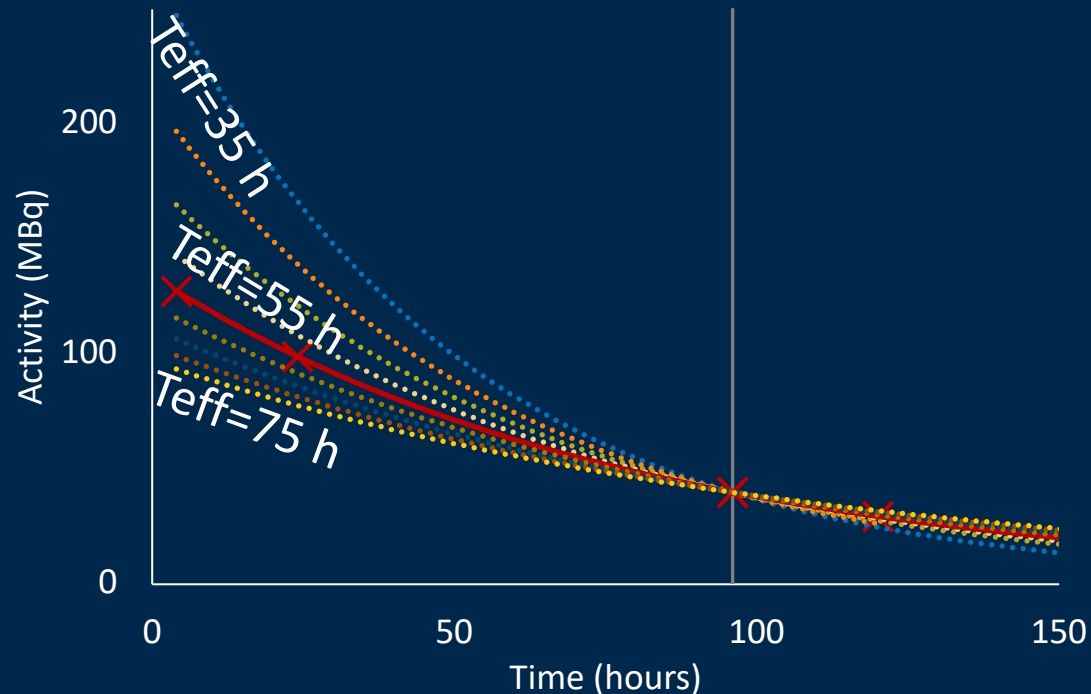
- Unlike in external radiotherapy, not standard practice in RPT
- Why?
  - Imaging burden
  - Lack of accurate and clinic friendly tools
  - Scarcity of well established dose - effects relationships
    - Potentially related to insufficient data
- Recent developments
  - Potential for reduced time point imaging-based dosimetry and faster scans
  - AI-based tools for segmentation
  - Publicly available & commercial tools for patient specific dosimetry



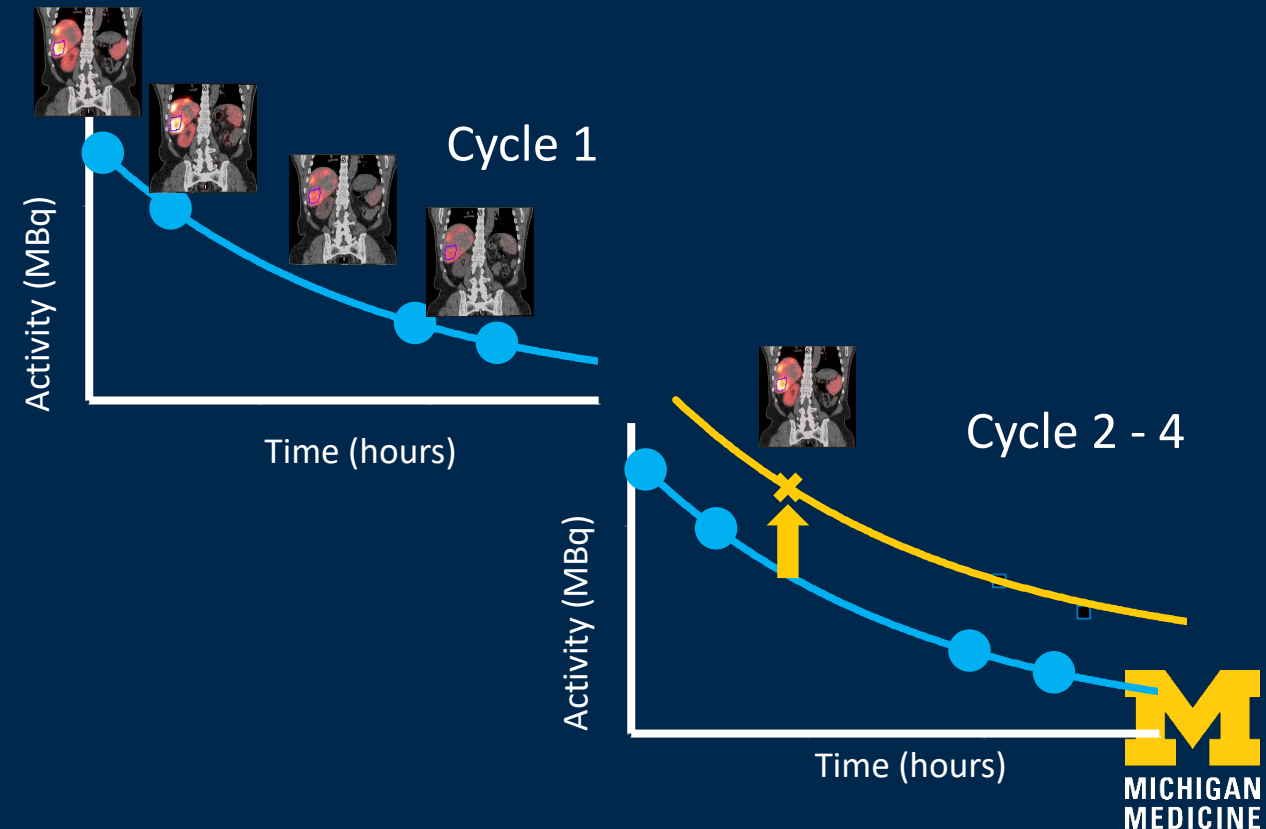
# Single time point methods to reduce imaging burden of dosimetry

- Why it works? Even wide variations in effective half-life gives similar TIA

$$\bar{D}(r_T) = \sum_{r_S} \tilde{A}(r_S) S(r_T \leftarrow r_S)$$

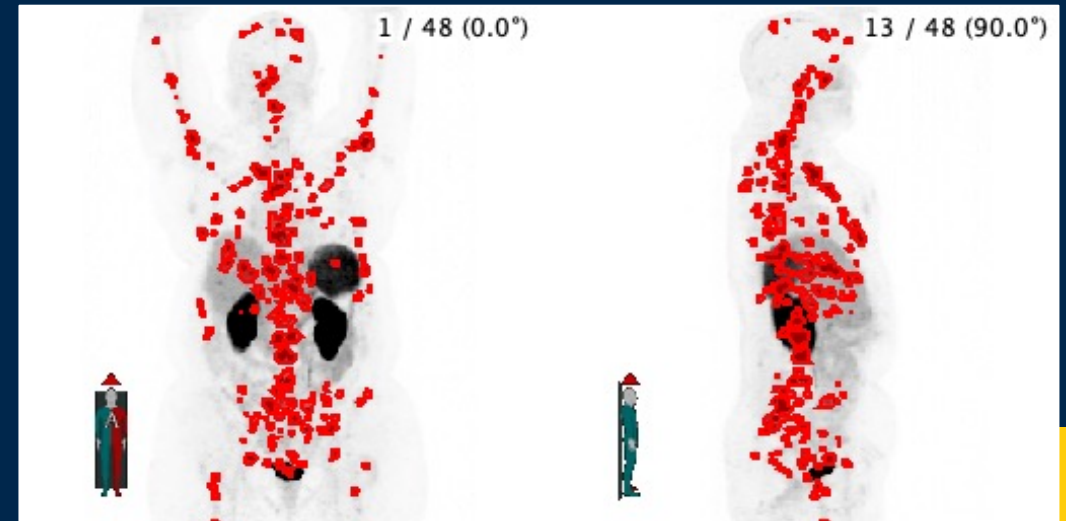
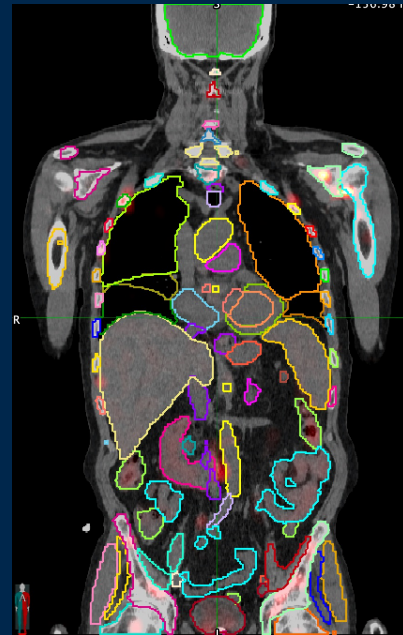


- Full Imaging in Cycle 1 + Single Timepoint at Others
  - Assumes kinetics are unchanged between cycles but allows for cycle specific changes in uptake



# Developments that facilitate patient specific dosimetry: AI-Segmentation

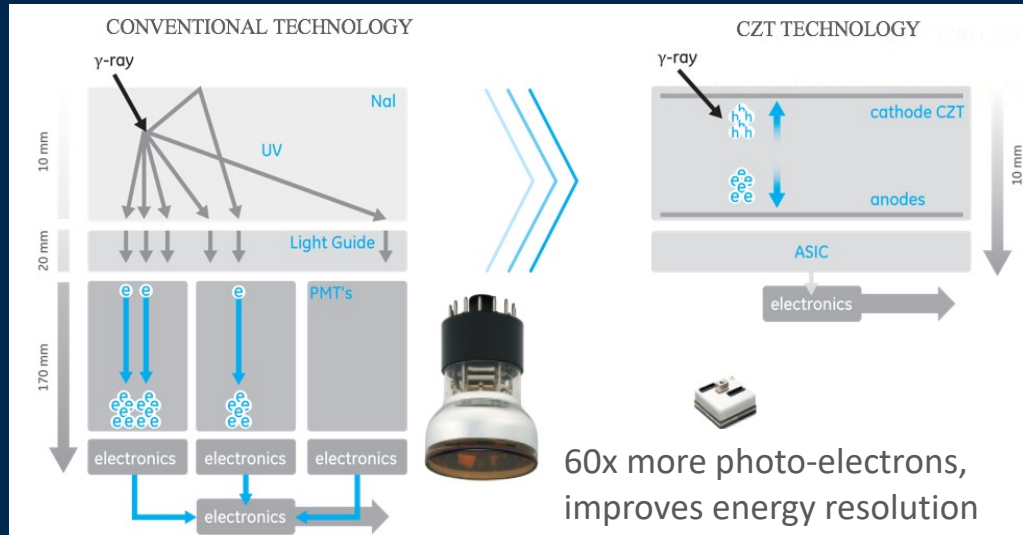
- Well-validated for normal organs
- Coupled with some dosimetry packages
- Individual lesion segmentation is more challenging
- Semi-automated tools available for whole-body tumor segmentation with and without AI for 'cleaning' physiological uptake



- Free-ware
  - TotalSegmentator:  
104 structures in CT
- <https://arxiv.org/pdf/2208.05868.pdf>

# Developments that facilitate dosimetry: Advances in SPECT & PET

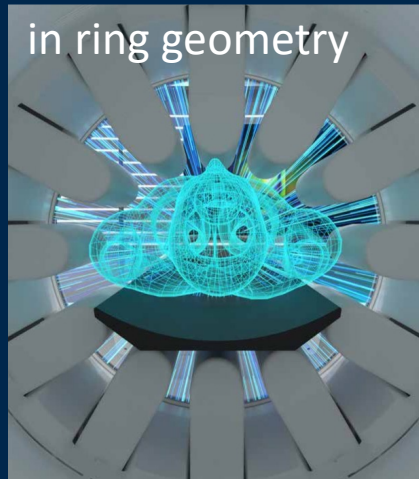
**SPECT:** Cadmium Zinc Telluride semiconductor for direct conversion of gamma energy to charge carriers



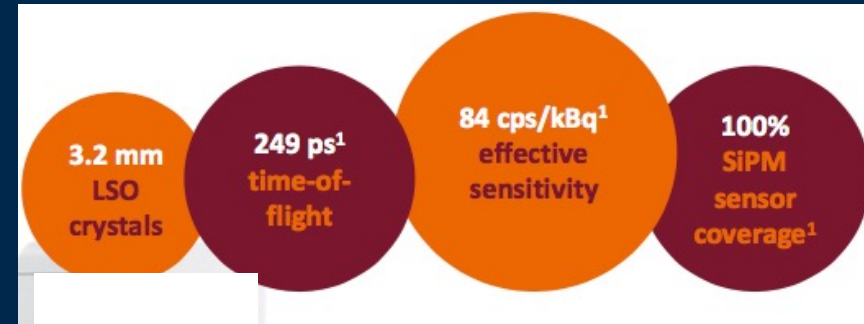
Built in source holders and calibration standards



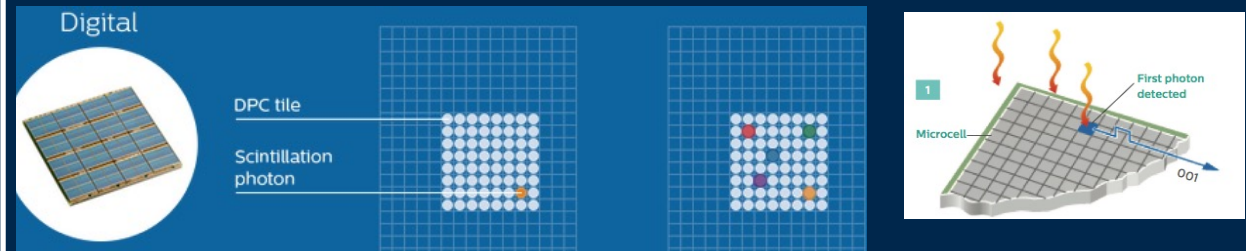
Multi-detectors in ring geometry



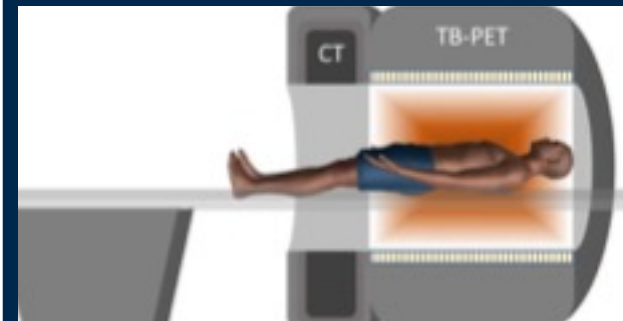
**PET** Si Photomultipliers. Reduced crystal size



Photon Counting Technology. Array of single photon avalanche diodes convert light from the scintillator directly to a digital signal



Total body PET. Gain in sensitivity:  
Improve SNR, reduce dose, or scan faster



Axial length

70 cm  
100 cm  
140 cm  
200 cm

Gain in body sensitivity  
(1-2-m-long object) vs 20 cm axial length

9-10 x  
15-20 x  
20-30 x  
30-40 x

# Developments that facilitate dosimetry: faster SPECT scans

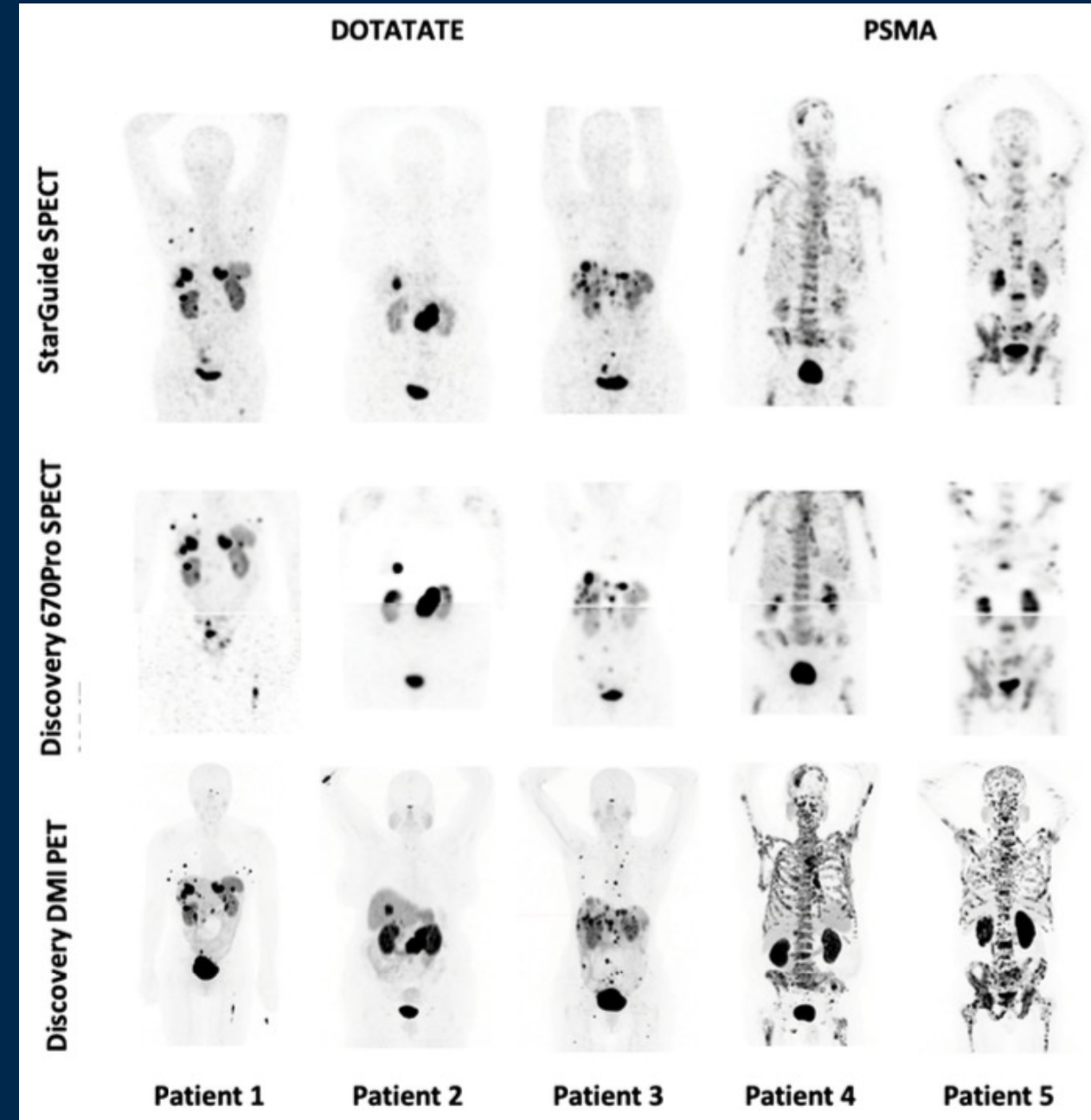
European Journal of Nuclear Medicine and Molecular Imaging  
<https://doi.org/10.1007/s00259-023-06176-6>

## ORIGINAL ARTICLE

### SPECT at the speed of PET: a feasibility study of CZT-based whole-body SPECT/CT in the post $^{177}\text{Lu}$ -DOTATATE and $^{177}\text{Lu}$ -PSMA617 setting

Hong Song<sup>1</sup> · Valentina Ferri<sup>1</sup> · Heying Duan<sup>1</sup> · Carina Mari Aparici<sup>1</sup> · Guido Davidzon<sup>1</sup> · Benjamin L. Franc<sup>1</sup> · Farshad Moradi<sup>1</sup> · Judy Nguyen<sup>1</sup> · Jagruti Shah<sup>1</sup> · Andrei Iagaru<sup>1</sup> 

- **New system:** Vertex to mid-thighs post-therapy SPECT/CT scans with 4 bed positions, 3 min/bed and a total scan time of **12 min**.
- **Old system:** 2 bed positions covering chest, abdomen, pelvis with total scan time of **32 min**.
- Scans acquired with faster scanning time using new system had **comparable** detection/targeting rate

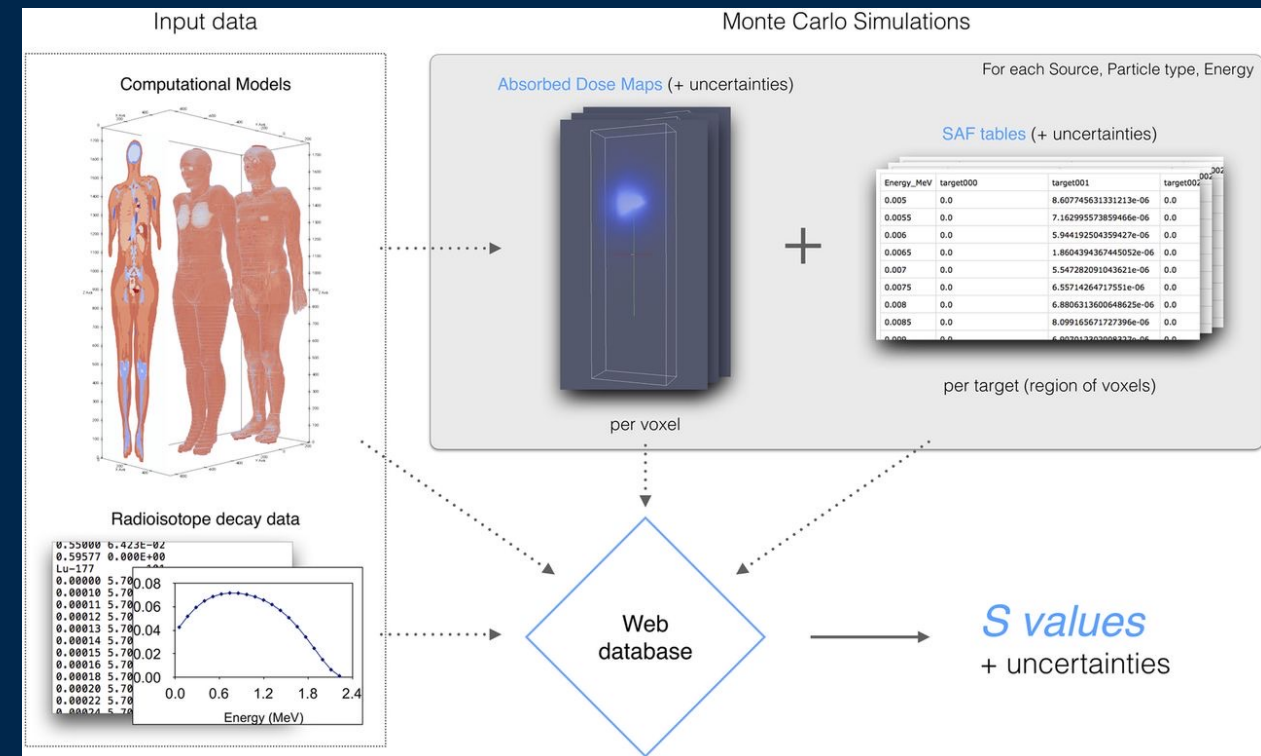




# Publicly Available Dosimetry Software

- MIRDsoft <https://mirdsoft.org/>

- OpenDose <https://www.opendose.org/>



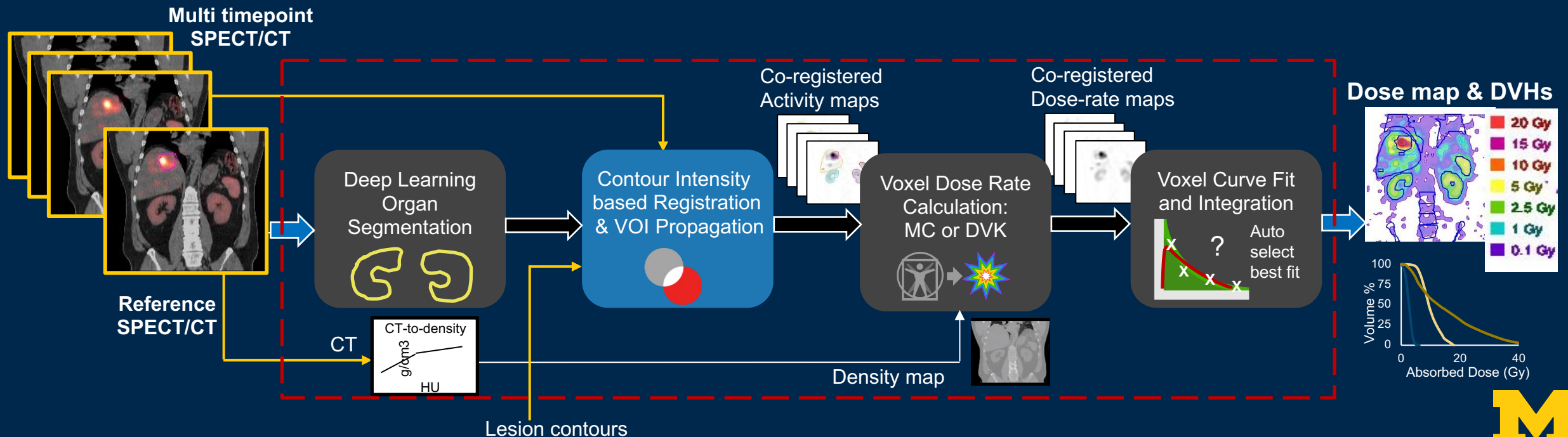
SAFs produced by MC simulations are stored in database along with input data. Web application allows calculation, and downloading of SAFs and S values

# Automated Monte Carlo voxel dosimetry in minutes

## A Pipeline for Automated Voxel Dosimetry: Application in Patients with Multi-SPECT/CT Imaging After $^{177}\text{Lu}$ -Peptide Receptor Radionuclide Therapy

J Nucl Med 2022; 63:1665–1672

Yuni K. Dewaraja<sup>1</sup>, David M. Mirando<sup>2</sup>, Avery B. Peterson<sup>1,3</sup>, Jeremy Niedbala<sup>1</sup>, John D. Millet<sup>1</sup>, Justin K. Mikell<sup>4</sup>, Kirk A. Frey<sup>1</sup>, Ka Kit Wong<sup>1</sup>, Scott J. Wilderman<sup>1</sup>, and Aaron S. Nelson<sup>2</sup>



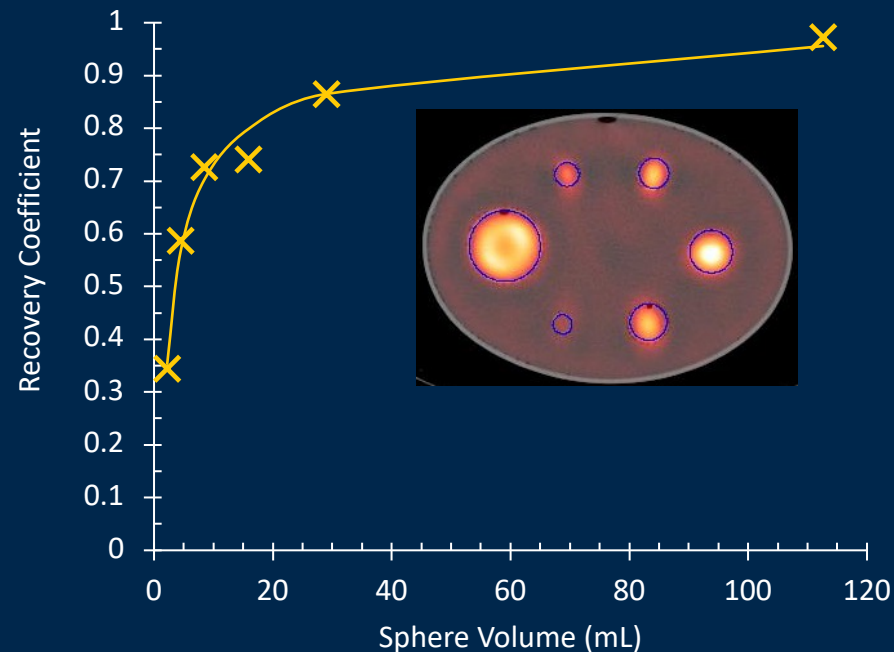
NCI R01CA240706. NIBIB R01EB022075



# Poor SPECT resolution remains a challenge

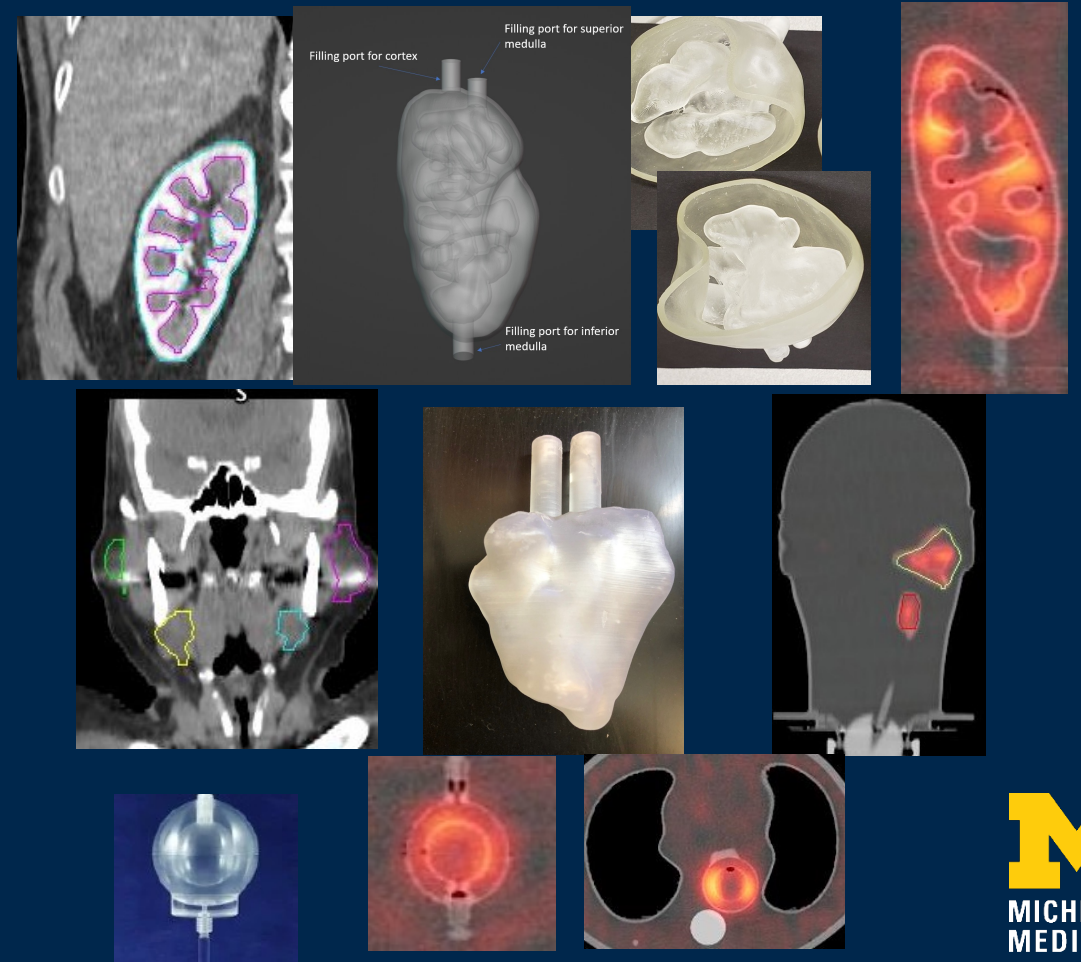
- Recovery Coefficients for Partial Volume Correction

- RC vs. volume curve using phantom meas.
- Practical, but limitations, specially for small/complex structures
- Mean value correction - not voxel level



- Structures in body are not spheres ...

- Limitations evident from phantom studies



# Absorbed Dose Estimation in RPT: What is possible & remaining challenges

- Image Acquisition
  - Reduced timepoints: Established for some therapies. Needed for others
  - Shorter scans: new detector systems & AI-based denoising
- Image Reconstruction, Quantification & Partial Volume Correction
  - Problematic for small/complex structures due to resolution and motion effects. Voxel-level PVC unresolved problem
  - Additional challenges when imaging alpha-emitters
- Organ/lesion Segmentation
  - Automated methods available for organs, under development for lesions
- Absorbed dose estimation
  - Multiple options including free-ware. Fast, accurate voxel-level calculation possible

Thank You  
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